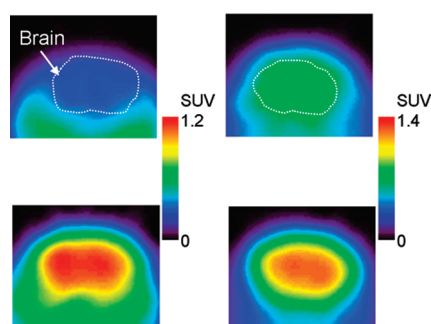


# *In Vivo* Evaluation of Limiting Brain Penetration of Probes for $\alpha_{2C}$ -Adrenoceptor Using Small-Animal Positron Emission Tomography

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## Abstract



To evaluate *in vivo* brain penetration of  $\alpha_{2C}$ -adrenoceptor ( $\alpha_{2C}$ -AR) antagonists as a therapeutic agent, we synthesized two new  $^{11}\text{C}$ -labeled selective  $\alpha_{2C}$ -AR antagonists 4-(6,7-dimethoxy-1,2,3,4-tetrahydroisoquinolin-2-yl)methyl-2-aryl-7-methoxybenzofuran ( $[^{11}\text{C}]\text{MBF}$ ) and acridin-9-yl-[4-(4-methylpiperazin-1-yl)phenyl]amine ( $[^{11}\text{C}]\text{JP-1302}$ ) as  $\alpha_{2C}$ -AR-selective positron emission tomography (PET) probes. The radiochemical yield, specific activity, and radiochemical purity of these probes was appropriate for injection. To evaluate whether the brain penetration of these probes is related to the function of two major drug efflux transporters, P-glycoprotein (P-gp) and breast cancer resistance protein (BCRP), we performed PET studies using wild-type and P-gp/Bcrp knockout mice. In wild-type mice, the radioactivity level after injection with  $[^{11}\text{C}]\text{MBF}$  initially increased and effluxed immediately from the brain, whereas that with  $[^{11}\text{C}]\text{JP-1302}$  was distributed throughout the brain. However, the regional distribution of radioactivity after injection with  $[^{11}\text{C}]\text{JP-1302}$  in the brain was different from that of  $\alpha_{2C}$ -ARs. In P-gp/Bcrp knockout mice, uptake of  $[^{11}\text{C}]\text{MBF}$  was approximately 3.7-fold higher and that of  $[^{11}\text{C}]\text{JP-1302}$  was approximately 1.6-fold higher than those in wild-type mice. These results indicate that brain penetration of the two PET probes was affected by modulation of P-gp and Bcrp functions.

**Keywords:**  $\alpha_{2C}$ -Adrenoceptor,  $^{11}\text{C}$ , 4-(6,7-dimethoxy-1,2,3,4-tetrahydroisoquinolin-2-yl)methyl-2-aryl-7-methoxybenzofuran (MBF), acridin-9-yl-[4-(4-methylpiperazin-1-yl)phenyl]amine (JP-1302), P-glycoprotein (P-gp), breast cancer resistance protein (Bcrp)

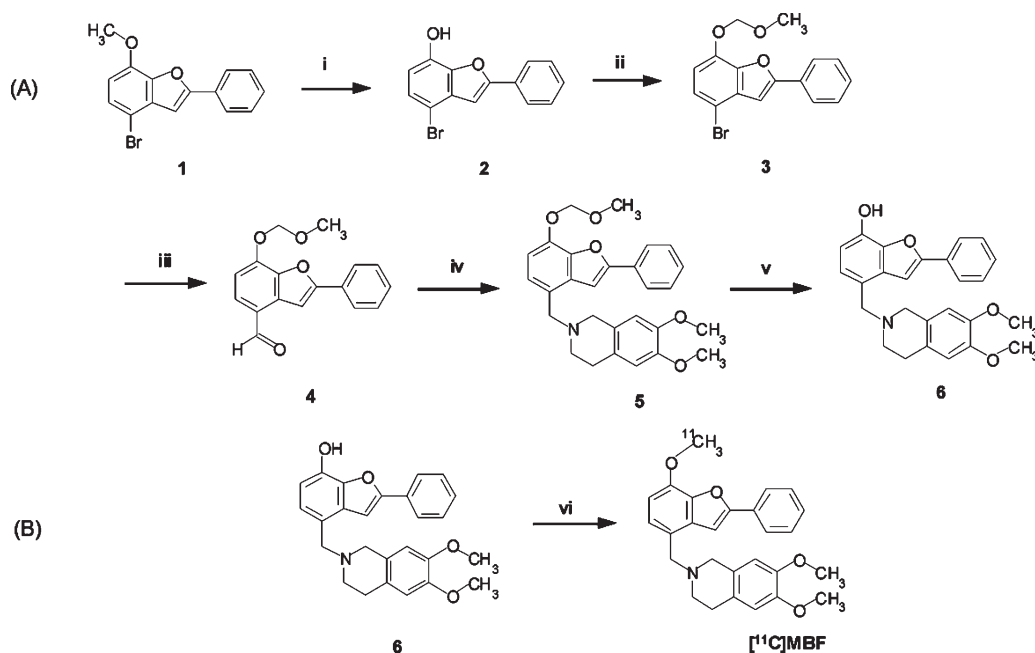
Drug efflux transporters are expressed at various protective organ and tissue surfaces and play a pivotal role in the absorption (small intestine), distribution (placenta and blood–brain barrier), and elimination (liver and small intestine) of xenobiotics. The most extensively characterized drug efflux transporters are the ATP-binding cassette (ABC) transporters, which include P-glycoprotein (P-gp), multidrug resistance-associated protein (MRP), and breast cancer resistance protein (BCRP) (1, 2). Some positron emission tomography (PET) probes for imaging the central nervous system (CNS) functions have revealed behavior as P-gp substrates (3–9). These PET probes showed a relatively rapid clearance of radioactivity from the brain; however, their uptake was noticeably enhanced by treatment with a P-gp inhibitor or modulator (8). To discern whether P-gp substrates are modulated by drug efflux transporters is important for development of new PET probes.

$\alpha_{2C}$ -Adrenoceptors ( $\alpha_{2C}$ -ARs) are a subtype of  $\alpha_2$ -ARs (10) and are feedback regulators of catecholamine release from adrenal chromaffin cells (11, 12). In the CNS, activation of  $\alpha_{2C}$ -ARs influences several complex memory and behavioral functions (13, 14). Involvement of  $\alpha_{2C}$ -ARs has been reported in hypothermic (15), locomotor (15, 16), cognitive (17), and analgesic effects (18, 19). In the mouse brain,  $\alpha_{2C}$ -ARs are present in the accumbens nuclei, caudate putamen, olfactory tubercles, lateral

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**Figure 1.** Synthesis of precursor 6 (A) and  $[^{11}\text{C}]$ MBF (B). Reagents and conditions: (i) boron tribromide,  $\text{CH}_2\text{Cl}_2$ ,  $0^\circ\text{C}$ , 2 h; (ii) chloromethyl methyl ether, *N,N'*-diisopropylethylamine,  $\text{CH}_2\text{Cl}_2$ , room temperature (rt), 4 h; (iii) normal butyl lithium, THF then DMF,  $-78^\circ\text{C}$  to rt, 1 h; (iv) 6,7-dimethoxy-1,2,3,4-tetrahydroisoquinoline hydrochloride, sodium tri(acetoxy)borohydride,  $\text{CH}_2\text{Cl}_2$ , rt, 16.5 h; (v) *p*-toluenesulfonic acid, methanol, rt, 7 h, 55.3% yield from 1, 98.7% chemical purity; (vi)  $[^{11}\text{C}]\text{CH}_3\text{I}$ , tetrabutylammonium hydroxide, DMF,  $80^\circ\text{C}$ , 5 min, 27% radiochemical yield (RCY) from  $[^{11}\text{C}]\text{CO}_2$ .

septum, hippocampus, amygdala, and frontal cortex (20, 21). To achieve a better understanding of the effects of  $\alpha_{2\text{C}}$ -ARs in CNS, selective probes with a high specificity that could detect low concentration sites would be valuable.

Although several PET probes for  $\alpha_2$ -ARs have been synthesized (22–26), a selective PET probe for  $\alpha_{2\text{C}}$ -ARs has not been synthesized until now. Recently, 4-(6,7-dimethoxy-1,2,3,4-tetrahydroisoquinolin-2-yl)methylbenzofuran derivatives were synthesized as selective  $\alpha_{2\text{C}}$ -ARs antagonists (27). Of these, 4-(6,7-dimethoxy-1,2,3,4-tetrahydroisoquinolin-2-yl)methyl-2-aryl-7-methoxybenzofuran (MBF) exhibited high and selective affinity for  $\alpha_{2\text{C}}$ -ARs ( $K_i$  for  $\alpha_{2\text{C}}$ , 20 nM;  $K_i$  for  $\alpha_{2\text{A}}$ , 1700 nM;  $K_i$  for  $\alpha_{2\text{B}}$ , 750 nM) (27). Furthermore, acridin-9-yl-[4-(4-methylpiperazin-1-yl)phenyl]amine (JP-1302) was recently synthesized and characterized as a selective  $\alpha_{2\text{C}}$ -AR antagonist ( $K_i$  for  $\alpha_{2\text{C}}$ , 28 nM;  $K_i$  for  $\alpha_{2\text{A}}$ , 3500 nM;  $K_i$  for  $\alpha_{2\text{B}}$ , 1500 nM;  $K_i$  for  $\alpha_{\text{D}}$ , 1700 nM) (28). Previous work with  $\alpha_2$ -AR ligands for CNS imaging agents showed that low nanomolar affinity is required (29), and general criteria for PET probes are proposed for lipophilicity ( $\log D < 3.5$ ) to predict brain penetration of PET probes (30). Calculated  $\log D$  values of MBF and JP-1302 were 5.72 and 5.13, respectively (Pallas 3.4, CompuDrug, Sedona, AZ). MBF and JP-1302 may be too lipophilic for imaging agents of central  $\alpha_{2\text{C}}$ -adrenoceptors due to few dozens of nanomolar affinity and relatively high  $\log D$  value. MBF and JP-1302 were

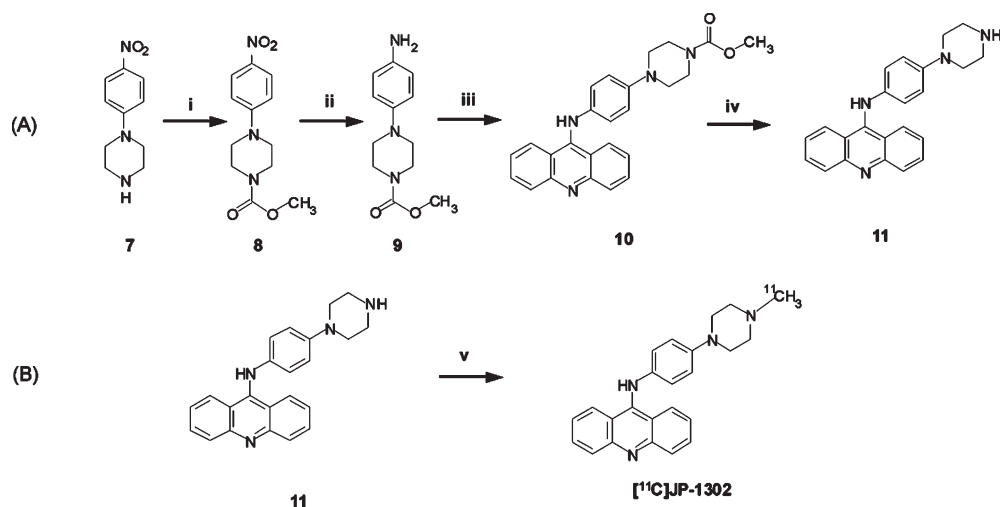
indicated as possible therapeutic agents for psychiatric and neurological disorders (27, 31). Here, we synthesized  $^{11}\text{C}$ -labeled MBF and JP-1302 as a PET probes to evaluate *in vivo* brain penetration of therapeutic agents and evaluated the P-gp and BCRP functions that mediated the brain penetration of these probes using small animal PET.

## Results and Discussion

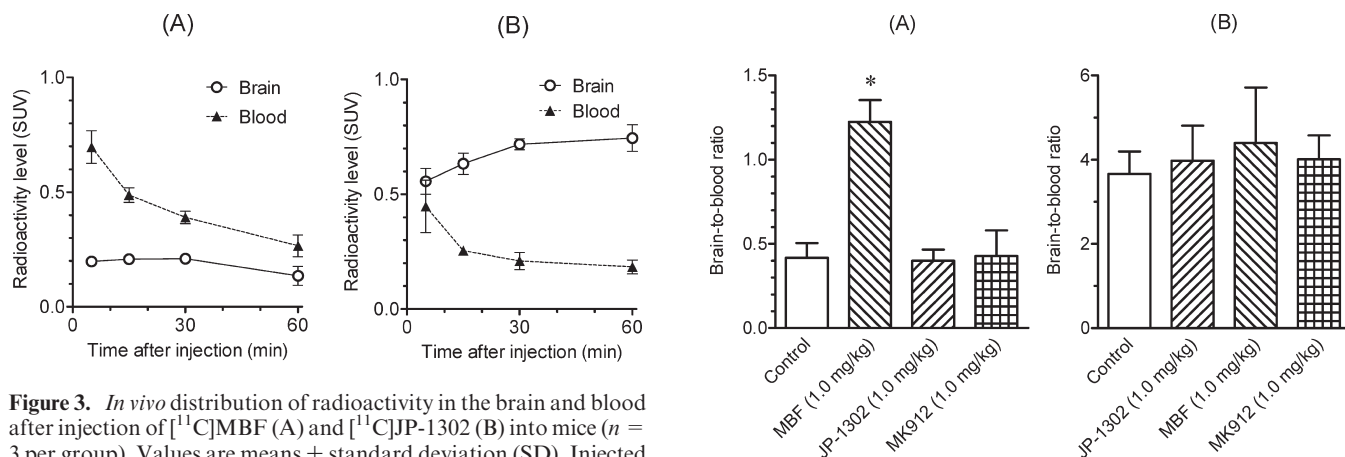
### Radiosynthesis of $[^{11}\text{C}]$ MBF and $[^{11}\text{C}]$ JP-1302

We successfully synthesized  $[^{11}\text{C}]$ MBF by methylation of the *O*-desmethyl precursor with  $[^{11}\text{C}]$ methyl iodide (Figure 1). The decay-corrected radiochemical yield of  $[^{11}\text{C}]$ MBF from  $[^{11}\text{C}]$ carbon dioxide was  $27\% \pm 4.7\%$  ( $n = 3$ ), and the specific activity was  $62 \pm 15$  TBq/mmol ( $n = 3$ ) at 30 min after the end of radionuclide production. The radiochemical yield and specific activity were applicable for injection as a PET probe. We achieved appropriate radiochemical purity ( $>97\%$ ) and stability of  $[^{11}\text{C}]$ MBF injection over 1 h after the end of synthesis (EOS).

We also successfully synthesized  $[^{11}\text{C}]$ JP-1302 by methylation of the *N*-desmethyl precursor with  $[^{11}\text{C}]$ methyl triflate (Figure 2). The decay-corrected radiochemical yield of  $[^{11}\text{C}]$ JP-1302 from  $[^{11}\text{C}]$ carbon dioxide was  $26\% \pm 5.8\%$  ( $n = 7$ ). As a result of the relatively low dose of precursor (0.2 mg), the radiochemical yield of  $[^{11}\text{C}]$ JP-1302 was the similar to that of  $[^{11}\text{C}]$ MBF, as achieved by methylation with  $[^{11}\text{C}]$ methyl iodide,



**Figure 2.** Synthesis of precursor **11** (A) and [ $^{11}\text{C}$ ]JP-1302 (B). Reagents and conditions: (i)  $\text{K}_2\text{CO}_3$ , methyl chloroformate,  $\text{CH}_2\text{Cl}_2$ , rt, 0.5 h; (ii) 10% Pd/C,  $\text{H}_2$ , ethanol, rt, 2 h; (iii) 9-chloroacridine, ethylene glycol, 150  $^\circ\text{C}$ , 1 h; (iv) KOH, water, ethylene glycol, rt, 150  $^\circ\text{C}$ , 4 h, 18.8% yield from **7**, 95.2% chemical purity; (v) [ $^{11}\text{C}$ ]methyl triflate, acetone, rt, 26% RCY from [ $^{11}\text{C}$ ]CO $_2$ .



**Figure 3.** *In vivo* distribution of radioactivity in the brain and blood after injection of [ $^{11}\text{C}$ ]MBF (A) and [ $^{11}\text{C}$ ]JP-1302 (B) into mice ( $n = 3$  per group). Values are means  $\pm$  standard deviation (SD). Injected dose of  $^{11}\text{C}$  ligands was 7.4–12 MBq/0.07–0.12 nmol. SUV, standardized uptake value.

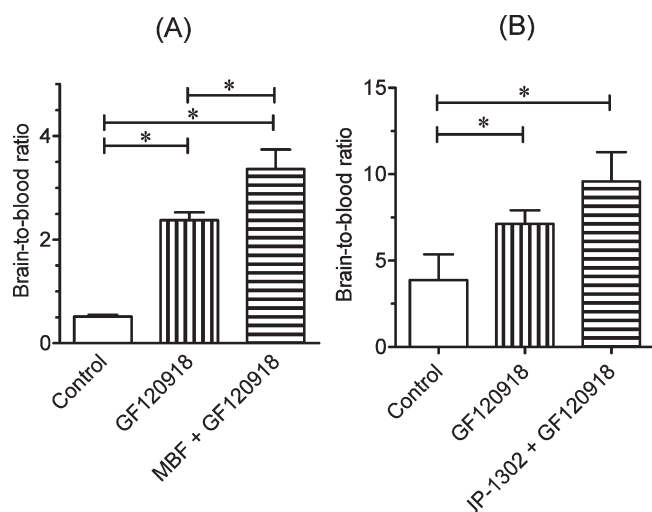
although the methylation with [ $^{11}\text{C}$ ]methyl triflate possibly improves the radiochemical yield (32). The specific activity was  $95 \pm 24$  TBq/mmol ( $n = 7$ ) at 30 min after the end of radionuclide production. The radiochemical yield and specific activity were suitable for injection as a PET probe. We achieved appropriate radiochemical purity (>96%) and stability of [ $^{11}\text{C}$ ]JP-1302 injection over 1 h after EOS.

### *In Vivo* Biodistribution in Mice

To evaluate *in vivo* brain penetration of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302, we investigated the time courses of radioactivity in the brain and blood after the injection of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 in normal mice (Figure 3). The radioactivity level of [ $^{11}\text{C}$ ]MBF in the brain was lower than that in the blood (Figure 3A), whereas the radioactivity level of [ $^{11}\text{C}$ ]JP-1302 in the brain was higher than that in the blood (Figure 3B). Next, we investigated specific

**Figure 4.** Effects of treatment with  $\alpha_{2C}$ -adrenoceptor ( $\alpha_{2C}$ -AR) ligands on the brain-to-blood ratio at 15 min after the injection of [ $^{11}\text{C}$ ]MBF or at 30 min after the injection of [ $^{11}\text{C}$ ]JP-1302 into mice ( $n = 3$ –7 per group). Values are means  $\pm$  SD. Injected dose of  $^{11}\text{C}$ -labeled ligands was 5.9–11 MBq/0.13–0.25 nmol. One of the  $\alpha_{2C}$ -AR ligands (MBF, JP-1302, MK912; 1.0 mg/kg) was intravenously co-injected with [ $^{11}\text{C}$ ]MBF or injected 15 min before administration of [ $^{11}\text{C}$ ]JP-1302. The \* indicates  $P < 0.05$  compared with control (one-way ANOVA and Dunnett's *post hoc* tests).

uptake of radioactivity by  $\alpha_{2C}$ -ARs in the brain by conducting a blocking study using cold MBF, cold JP-1302, and the high-affinity  $\alpha_{2C}$ -AR antagonist MK-912 ((2*S*, 12*bS*)1',3'-dimethylspiro(1,3,4,5',6,6',7,12*b*-octahydro-2*H*-benzo[*b*]furo[2,3-*a*]quinolizine)-2,4'-pyrimidin-2'-one,  $K_i$  for  $\alpha_{2C} = 0.03$  nM) (22) (Figure 4). Treatment with any investigated  $\alpha_{2C}$ -AR ligands did not affect the brain-to-blood ratio of [ $^{11}\text{C}$ ]JP-1302 (Figure 4B). Therefore, the uptake of [ $^{11}\text{C}$ ]JP-1302 in the brain may be nonspecific. On the other hand, the treatment with cold MBF induced a significant increase in the brain-to-blood ratio of [ $^{11}\text{C}$ ]MBF, although the brain-to-blood ratio of [ $^{11}\text{C}$ ]MBF was



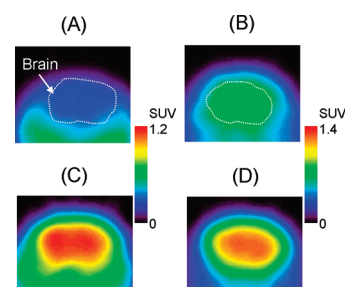
**Figure 5.** Effects of the inhibition of P-gp and Bcrp functions on the brain-to-blood ratio at 30 min after the injection of [ $^{11}\text{C}$ ]MBF (A) and [ $^{11}\text{C}$ ]JP-1302 (B). The  $^{11}\text{C}$ -labeled ligands (11–12 MBq/0.12–0.17 nmol), P-gp/BCRP inhibitor GF120918 (5.0 mg/kg), or cold ligand (MBF or JP-1302; 1.0 mg/kg) were intravenously co-injected into mice ( $n = 4$  per group). Values are means  $\pm$  SD; \* indicates  $P < 0.05$  (one-way ANOVA and Bonferroni's multiple comparison tests).

not affected by the treatment with cold JP-1302 and MK-912 (Figure 4A). Furthermore, treatment with the P-gp/BCRP inhibitor GF120918 induced a significant increase in the brain-to-blood ratio of [ $^{11}\text{C}$ ]MBF, and treatment with GF120918 plus cold MBF induced a significant increase in the brain-to-blood ratio compared with treatment with GF120918 alone (Figure 5A). These results suggest that the penetration of [ $^{11}\text{C}$ ]MBF and cold MBF into the brain is related to the function of drug efflux transporters as a substrate. Unexpectedly, the treatment with GF120918 induced a significant increase in the brain-to-blood ratio of [ $^{11}\text{C}$ ]JP-1302 (Figure 5B). These results suggested that the penetration of [ $^{11}\text{C}$ ]JP-1302 into the brain is also related to the function of drug efflux transporters as a substrate.

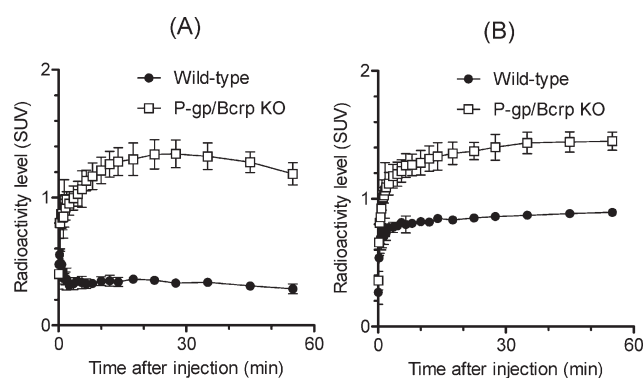
### Metabolites Analysis in the Brain and Plasma of Mice

The percentages of the unchanged of [ $^{11}\text{C}$ ]MBF in the brain and plasma at 30 min after the injection were  $88.4\% \pm 6.3\%$  and  $84.0\% \pm 6.8\%$ , respectively ( $n = 3$ ). [ $^{11}\text{C}$ ]MBF demonstrated a high metabolic stability at 30 min after injection. A radiolabeled metabolite with high polarity was observed on HPLC charts (retention time, 2.5 min).

The percentages of unchanged [ $^{11}\text{C}$ ]JP-1302 in the brain and plasma at 30 min after the injection were  $88.4\% \pm 1.8\%$  and  $17.4\% \pm 5.9\%$ , respectively ( $n = 4$ ). Therefore, [ $^{11}\text{C}$ ]JP-1302 seemed to readily metabolize in peripheral organs. A radiolabeled metabolite with high polarity was observed on HPLC charts (retention time, 2.5 min).



**Figure 6.** Typical transaxial positron emission tomography (PET) images showing [ $^{11}\text{C}$ ]MBF (A, C) and [ $^{11}\text{C}$ ]JP-1302 (B, D) in the brain of a wild-type mouse (A, B) and a P-gp/Bcrp knockout mouse (C, D). Injected dose was 3.7–4.7 MBq/0.071–0.56 nmol. PET images were acquired from 5 to 60 min after the injection. Mice were anesthetized with isoflurane and fixed in a prone position on the bed of the scanner.



**Figure 7.** Time–activity curves of the brain after injection of [ $^{11}\text{C}$ ]MBF (A) and [ $^{11}\text{C}$ ]JP-1302 (B) in wild-type mice and P-gp/Bcrp knockout mice ( $n = 3$  per group). Values are means  $\pm$  SD. The injected dose was 3.6–8.1 MBq/0.033–1.22 nmol. SUV, standardized uptake value.

### PET Studies in Wild-Type and P-gp/Bcrp Knockout Mice

To evaluate whether the brain penetration by [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 is related to P-gp and Bcrp functions, we further performed PET studies using [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 in P-gp/Bcrp knockout and wild-type mice (Figures 6 and 7). In wild-type mice after injection with [ $^{11}\text{C}$ ]MBF, the radioactivity level was low in the brain (Figure 6A). In P-gp/Bcrp knockout mice after injection with [ $^{11}\text{C}$ ]MBF, the radioactivity level was distributed throughout the brain (Figure 6C); however, the regional distribution of radioactivity in the brain was different from that of  $\alpha_2\text{-ARs}$  (20, 21). The radioactivity level in the wild-type and P-gp/Bcrp knockout mice after injection with [ $^{11}\text{C}$ ]JP-1302 was also distributed throughout the brain (Figure 6B,D), and it initially increased and then remained constant (Figure 7B). This result indicates that [ $^{11}\text{C}$ ]JP-1302 may bind nonspecifically and irreversibly in the brain and suggests that [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 are inadequate for evaluation of  $\alpha_2\text{-ARs}$  in the brain. In P-gp/Bcrp knockout mice after injection with [ $^{11}\text{C}$ ]MBF, the radioactivity level in the brain increased gradually after initial uptake for 20 min after

injection and then decreased (Figure 7A). The area under the time–activity curve of the region of interest in the brain from 0 to 60 min after the injection ( $AUC_{\text{brain}[0-60\text{min}]}$ ) in P-gp/Bcrp knockout mice was approximately 3.7-fold higher than that in wild-type mice ( $74.4 \pm 6.0$  in P-gp/Bcrp knockout mice and  $19.8 \pm 0.8$  in wild-type mice;  $n = 3$  each group). These results suggested effective exclusion of [ $^{11}\text{C}$ ]MBF from the brain by P-gp and Bcrp function-mediated drug efflux. In P-gp/Bcrp knockout mice after injection with [ $^{11}\text{C}$ ]JP-1302, the kinetics of radioactivity in the brain followed a time course similar to that in wild-type mice after injection with [ $^{11}\text{C}$ ]JP-1302, but the radioactivity level was higher than that in wild-type mouse (Figure 7B). The  $AUC_{\text{brain}[0-60\text{min}]}$  in P-gp/Bcrp knockout mice was approximately 1.6-fold higher than that in wild-type mice ( $82.1 \pm 4.9$  in P-gp/Bcrp knockout mice;  $51.0 \pm 0.7$  in wild-type mice;  $n = 3$  each group). These results suggest that brain penetration of [ $^{11}\text{C}$ ]JP-1302 is mediated by P-gp and Bcrp functions.

Consequently, [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 are inadequate for evaluation of the function of  $\alpha_{2\text{C}}$ -AR in the brain as PET probes due to the effect of drug efflux transporters. As recent evidence from P-gp and Bcrp knockout mice suggests (33), PET study using P-gp/Bcrp knockout mice is more effective than that using P-gp knockout or Bcrp knockout mice alone to study brain penetration of probes related to P-gp and Bcrp functions (34–36). Therefore, PET study using P-gp/Bcrp knockout mice is more useful for evaluating the P-gp and Bcrp function-mediated brain penetration of PET probes.

## Conclusions

We reliably synthesized [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 as a PET probes to evaluate *in vivo* brain penetration of  $\alpha_{2\text{C}}$ -adrenoceptor antagonists as therapeutic agents. Brain penetration of these two PET probes was affected by modulation of drug efflux transporter functions. We also proposed that PET study using P-gp/Bcrp knockout mice is more useful for evaluating the P-gp and Bcrp function-mediated brain penetration of PET probes.

## Methods

### General

Reagents and organic solvents were commercially available and used without further purification. JP-1302 dihydrochloride was purchased from Tocris Bioscience (Bristol, U.K.). MBF was prepared in our laboratory as described previously (27) with some modifications. GF120918 was prepared in our laboratory as described previously (37, 38) with some modifications.

Proton nuclear magnetic resonance ( $^1\text{H}$  NMR) and carbon-13 nuclear magnetic resonance ( $^{13}\text{C}$  NMR) spectra were

recorded on the JNM-AL300 spectrometer (Jeol, Tokyo, Japan) or the JNM-GX-270 spectrometer (Jeol). High-resolution mass spectra (MS) were obtained on the JEOL NMS-SX 102-SX spectrometer (Jeol). Column chromatography was carried out using Kieselgel gel 60 F<sub>254</sub> (70–230 mesh; Merck, Darmstadt, Germany) or Wakogel C-200 (100–200 mesh; Wako Pure Chemical Industries, Osaka, Japan).

Male FVB mice were purchased from CLEA Japan (Tokyo, Japan). Male P-gp/Bcrp knockout [*Mdr1a/1b*(–/–)-*Abcg2*(–/–)] mice (39) were purchased from Taconic Farm (Hudson, NY). The animals were maintained and handled in accordance with the recommendations by the US National Institutes of Health and in-house guidelines (National Institute of Radiological Sciences, Chiba, Japan). The animal experiments were approved by the Animal Ethics Committee of the National Institute of Radiological Sciences.

### Synthesis of 4-(6,7-Dimethoxy-1,2,3,4-tetrahydroisoquinoline-2-ylmethyl)-2-phenylbenzofuran-7-ol (6)

Boron tribromide in dichloromethane (1.0 M, 20 mL, 20 mmol) was added to a solution of 4-bromo-7-methoxy-2-phenyl-2,3-dihydrobenzofuran (**1**, 0.86 g, 2.8 mmol) (**27**) in dichloromethane (71 mL) at 0 °C and stirred for 2 h. The mixture was poured into a saturated solution of monopotassium phosphate and extracted with diethyl ether. The organic layer was washed with brine, dried over sodium sulfate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane and ethyl acetate (5:1, v/v) as the mobile phase, yielding 4-bromo-2-phenylbenzofuran-7-ol (**2**; 0.73 g, 2.5 mmol) as a white-colored solid.

*N,N'*-Diisopropylethylamine (0.05 mL, 0.27 mmol) and chloromethyl methyl ether (0.02 mL, 0.27 mmol) were added to a solution of compound **2** (0.053 g, 0.18 mmol) in dichloromethane (3.6 mL). The solution was warmed to ambient temperature and stirred for 4 h. The reaction was quenched with a saturated solution of ammonium chloride and extracted with dichloromethane. The organic layer was washed with brine, dried over sodium sulfate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane ethyl acetate (10:1, v/v) as the mobile phase, yielding 4-bromo-7-(methoxymethoxy)-2-phenylbenzofuran (**3**; 0.059 g, 0.18 mmol) as a yellow-colored solid.

Normal butyl lithium (1.6 M in hexane 1.3 mL, 2.07 mmol) and *N,N*-dimethylformamide (DMF) (0.21 mL, 2.76 mmol) were added to a solution of compound **3** (0.46 g, 1.38 mmol) in tetrahydrofuran (14 mL) at –78 °C. The solution was warmed to ambient temperature and stirred for 1 h. The reaction mixture was quenched with water and extracted with ethyl acetate. The organic layer was washed with brine, dried over sodium sulfate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane and ethyl acetate (from 10:1 [v/v] to 5:1 [v/v], gradient elution) as the mobile phase, yielding 7-(methoxymethoxy)-2-phenylbenzofuran-4-carbaldehyde (**4**; 0.34 g, 1.22 mmol) as a white-colored solid.

6,7-Dimethoxy-1,2,3,4-tetrahydroisoquinoline hydrochloride (0.25 g, 1.06 mmol) and sodium tri(acetoxy)borohydride (0.40 g, 1.77 mmol) were added to a solution of compound **4** (0.25 g, 0.89 mmol) in 1,2-dichloroethane (7.4 mL) at 0 °C.

The solution was warmed to ambient temperature and stirred for 16.5 h. The reaction mixture was quenched with 1 M sodium hydroxide and extracted with dichloromethane. The organic layer was washed with brine, dried over potassium carbonate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane and ethyl acetate (1:1, v/v) as the mobile phase, yielding 4-(6,7-dimethoxy-1,2,3,4-tetrahydroisoquinoline-2-ylmethyl)-7-methoxymethoxy-2-phenylbenzofuran (**5**; 0.324 g, 0.71 mmol) as a white-colored solid.

*p*-Toluenesulfonic acid (0.067 g, 0.35 mmol) was added to a solution of compound **5** (0.027 g, 0.059 mmol) in methanol (3.0 mL). After the mixture was stirred for 7 h, the solvent was evaporated. The residue was suspended in dichloromethane, made basic using 28% ammonia–water, and extracted with dichloromethane. The organic layer was washed with brine, dried over sodium sulfate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane and ethyl acetate (1:2, v/v) as the mobile phase, yielding compound **6** (0.022 g, 0.054 mmol, 55.3% from **1**) as a yellow-colored solid. <sup>1</sup>H NMR (300 MHz, CDCl<sub>3</sub>): δ (ppm) 2.87 (4H, s), 3.68 (2H, s), 3.79 (3H, s), 3.83 (3H, s), 3.85 (2H, s), 6.48 (1H, s), 6.59 (1H, s), 6.64 (1H, d, *J* = 7.80 Hz), 7.02 (1H, d, *J* = 7.80 Hz), 7.14 (1H, s), 7.28 (1H, brt), 7.37 (2H, brt), 7.78 (2H, d, *J* = 7.20 Hz). <sup>13</sup>C NMR (75.5 MHz, CDCl<sub>3</sub>): δ (ppm) 27.70, 50.62, 55.12, 55.82, 55.84, 59.04, 100.87, 109.45, 111.17, 111.24, 120.71, 124.89, 125.11, 125.58, 125.70, 128.30, 128.51, 130.23, 130.90, 141.27, 143.78, 147.24, 147.57, 155.51. High-resolution MS *m/z*: 416.1862 (calculated for C<sub>26</sub>H<sub>25</sub>NO<sub>4</sub>, 416.4967). Chemical purity: 98.7% (Supporting Information).

### Synthesis of Acridin-9-yl-[4-(piperazin-1-yl)phenyl]-amine (**11**)

Potassium carbonate (0.47 g, 3.4 mmol) and methyl chloroformate (0.2 mL, 2.6 mmol) were added a solution of 1-(4-nitrophenyl)piperazine (**7**; 0.35 g, 1.7 mmol) in dichloromethane (7 mL) at room temperature (rt). The resulting solution was stirred for 30 min, and 1 M sodium hydroxide (5 mL) was added at rt. The reaction mixture was extracted with dichloromethane. The organic layer was dried with sodium sulfate and evaporated *in vacuo*. The residue was purified by column chromatography on silica gel using a mixture of dichloromethane and methanol (9:1, v/v) as the mobile phase, yielding 4-(4-nitrophenyl)piperazine-1-carboxylate (**8**; 0.45 g, 1.7 mmol) as a yellow-colored solid.

Compound **8** (0.15 g, 0.57 mmol) was dissolved in ethanol (5 mL) and tetrahydrofuran (3.5 mL). The solution was purged with hydrogen gas, and 10% palladium carbon (70 mg) was added. The resulting solution was stirred for 2 h under hydrogen gas and then filtered. The filtrate was condensed and purified by column chromatography on silica gel using a mixture of dichloromethane and methanol (9:1, v/v) as the mobile phase, yielding methyl 4-(4-aminophenyl)piperazine-1-carboxylate (**9**; 67 mg, 0.29 mmol) as a white-colored solid.

Compound **9** (0.80 g, 3.4 mmol) was dissolved in ethylene glycol (20 mL). The solution was heated to 150 °C and 9-chloroacridine (0.87 g, 4.1 mmol) was added. The resulting solution was stirred for 1 h. The solution was condensed and

added to a mixture of ethyl acetate and water. The extraction was carried out with ethyl acetate. The organic layer was dried with sodium sulfate, and concentrated. The residue was purified by column chromatography on silica gel using a mixture of *n*-hexane and ethyl acetate (1:1, v/v) as the mobile phase, yielding 4-(4-(acridin-9-ylamino)phenyl)piperazine-1-carboxylate (**10**; 0.90 g, 2.2 mmol) as an orange-colored solid.

Compound **10** (0.10 g, 0.25 mmol) was dissolved in ethylene glycol (5 mL). The resulting solution was heated to 150 °C; potassium hydroxide solution (0.18 mg/15 mL, 3.2 mmol) was dropped into the solution and stirred for 4 h. The solution was condensed and was added to a mixture of dichloromethane and water. The mixture was extracted with dichloromethane. The organic layer was dried with sodium sulfate and concentrated. The residue was purified by column chromatography on silica gel using a mixture of dichloromethane and methanol (9:1, v/v) as the mobile phase, yielding compound **11** (41 mg, 0.12 mmol, 18.8% from **7**) as an orange-colored solid. <sup>1</sup>H NMR (300 MHz, CDCl<sub>3</sub>): δ (ppm) 7.97 (4H, m, Ar–H), 7.62 (2H, m, Ar–H), 7.26 (2H, m, Ar–H), 6.89 (4H, m), 3.11 (4H, m), 3.08 (4H, m). High-resolution MS *m/z*: 355.1912 (calculated for C<sub>23</sub>H<sub>22</sub>N<sub>4</sub>, 355.4624). Chemical purity: 95.2% (Supporting Information).

### Radiosynthesis of [<sup>11</sup>C]MBF

<sup>11</sup>C was produced by <sup>14</sup>N(p, α)<sup>11</sup>C nuclear reaction using a CYPRIS HM-18 cyclotron (Sumitomo Heavy Industries, Tokyo, Japan). [<sup>11</sup>C]Methyl iodide was prepared from [<sup>11</sup>C]carbon dioxide via [<sup>11</sup>C]methanol using an automated system as described previously (*40*). [<sup>11</sup>C]Methyl iodide was trapped in the solution of DMF (0.35 mL) containing desmethyl MBF (1.0 mg) and 1.0 M tetrabutylammonium hydroxide in methanol (3 μL) on cooling, and the solution was then heated to 80 °C for 5 min. After cooling again, 0.5 mL of eluent for the preparative high-performance liquid chromatography (HPLC) was added, and the reaction mixture was applied to the preparative HPLC. Preparative HPLC was carried out using a Capcell Pak C18 UG 80 column (10 mm internal diameter × 250 mm length; Shiseido, Tokyo, Japan) with an ultraviolet detector at 254 nm and a radioactivity detector. Elution was carried out using a mixture of acetonitrile and 0.1 M ammonium formate (80:20, v/v/v) as the mobile phase at a flow rate of 5 mL/min. The retention times of desmethyl MBF and [<sup>11</sup>C]MBF were 4.5 and 7.5 min, respectively. The HPLC fraction of [<sup>11</sup>C]MBF was collected into a flask to which 25% ascorbic acid (100 μL) and Tween 80 (75 μL) in ethanol (0.3 mL) had been added before radiosynthesis, and then evaporated to dryness. The residue was dissolved in physiological saline.

The products were analyzed by HPLC using a Capcell Pak C18 UG 80 column (4.6 mm internal diameter × 250 mm length; Shiseido). Elution was carried out using the same mobile phase as that used for preparative HPLC at a flow rate of 2.0 mL/min. The retention time of [<sup>11</sup>C]MBF was 3.4 min.

### Radiosynthesis of [<sup>11</sup>C]JP-1302

[<sup>11</sup>C]Methyl iodide was prepared as described above. [<sup>11</sup>C]Methyl iodide was passed through a glass column containing silver triflate at 180 °C with a nitrogen gas flow to convert it into [<sup>11</sup>C]methyl triflate. This [<sup>11</sup>C]methyl triflate

was trapped in the solution of acetone (0.3 mL) containing desmethyl JP-1302 (0.3 mg) at rt. After cooling, 0.5 mL of eluent for the preparative HPLC was added, and the reaction mixture was applied to the preparative HPLC. Preparative HPLC was carried out using a Capcell Pak C18 UG 80 column (10 mm internal diameter  $\times$  250 mm length; Shiseido) with an ultraviolet detector at 254 nm and a radioactivity detector. Elution was carried out using a mixture of acetonitrile and 0.1% triethylamine in water (50:50, v/v/v) as the mobile phase at a flow rate of 5 mL/min. The retention time of desmethyl JP-1302 and [ $^{11}\text{C}$ ]JP-1302 were 5.5 and 8.5 min, respectively. The HPLC fraction of [ $^{11}\text{C}$ ]JP-1302 was collected into a flask to which 25% ascorbic acid (100  $\mu\text{L}$ ) and Tween 80 (75  $\mu\text{L}$ ) in ethanol (0.3 mL) had been added before radiosynthesis and then evaporated to dryness. The residue was dissolved in physiological saline.

The products were analyzed by HPLC using an X Bridge C18 column (4.6 mm internal diameter  $\times$  150 mm length; Waters, Milford, MA). Elution was carried out using a mixture of acetonitrile and 0.1% triethylamine in water (40:60, v/v/v) as the mobile phase at a flow rate of 1.5 mL/min. The retention time of [ $^{11}\text{C}$ ]JP-1302 was 4.0 min.

### **In Vivo Biodistribution in Mice**

The tissue distribution of radioactivity after the injection of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 was investigated. The  $^{11}\text{C}$ -labeled ligand (7.4–12 MBq/0.07–0.12 nmol) was intravenously injected into normal mice (age, 7 weeks). Mice were sacrificed by cervical dislocation at 5, 15, 30, or 60 min after injection ( $n = 3$  per group).

The effects of treatment with a cold  $\alpha_2\text{C}$ -AR ligand on tissue distribution of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 were investigated. The  $^{11}\text{C}$ -labeled ligand (5.9–11 MBq/0.13–0.25 nmol) was intravenously injected into normal mice (age, 8–10 weeks,  $n = 3$ –7 per group). One of the  $\alpha_2\text{C}$ -AR ligands (MBF, JP-1302, MK912; dose, 1.0 mg/kg) was intravenously co-injected with [ $^{11}\text{C}$ ]MBF or injected 15 min before administration of [ $^{11}\text{C}$ ]JP-1302. Mice were sacrificed by cervical dislocation at 15 min ([ $^{11}\text{C}$ ]MBF) or 30 min ([ $^{11}\text{C}$ ]JP-1302) after the injection.

The effects of the inhibition of P-gp and Bcrp functions on tissue distribution of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 were investigated. The  $^{11}\text{C}$ -labeled ligand (11–12 MBq/0.12–0.17 nmol), P-gp/BCRP inhibitor GF120918 (5.0 mg/kg), or cold ligand (MBF or JP-1302; 1.0 mg/kg) were intravenously co-injected into mice (age, 7–8 weeks,  $n = 4$  per group). Mice were sacrificed by cervical dislocation at 30 min after the injection.

Blood samples were collected by heart puncture, and the tissues were dissected out and weighed. Radioactivity in samples was measured using an automatic gamma counter (Wizard 3" 1480, PerkinElmer, Waltham, MA). Tissue uptake of  $^{11}\text{C}$  was expressed as the standardized uptake value [SUV, (tissue radioactivity/gram or milliliter of tissue)/(injected radioactivity/gram of body weight)].

### **Metabolite Analysis in the Brain and Plasma of Mice**

[ $^{11}\text{C}$ ]MBF (44 MBq/1.5 nmol) or [ $^{11}\text{C}$ ]JP1302 (59 MBq/1.3 nmol) was intravenously injected into male ddY mice (age, 9 weeks; weight, 35–41 g;  $n = 3$ –4 per tracer). Mice were sacrificed by cervical dislocation at 30 min after the injection. Blood samples were collected by heart puncture into a heparinized syringe, and the whole brain was dissected out.

Deproteinization was carried out using previously described methods (34–36) mentioned below. Plasma and homogenized brain tissues were deproteinized with the same volume of ice-cold acetonitrile. The mixture was then vortexed and centrifuged at 20 000g for 2 min, and the supernatant was collected. Supernatants were analyzed using HPLC with a radioactivity detector (41) and an ultraviolet detector at 254 nm on a Novapak C18 column (100 mm internal diameter  $\times$  8 mm length; Waters, Milford, MA) contained within a radial compression module (RCM-100, Waters) for [ $^{11}\text{C}$ ]MBF or a Capcell Pak C18 UG 80 column (4.6 mm internal diameter  $\times$  250 mm length; Shiseido) for [ $^{11}\text{C}$ ]JP-1302. Elution was carried out using a mixture of acetonitrile and 0.1% triethylamine in water (50:50, v/v) for [ $^{11}\text{C}$ ]MBF or a mixture of methanol and 50 mM sodium acetate buffer (80:20, v/v) for [ $^{11}\text{C}$ ]JP-1302 at a flow rate of 1.5 mL/min. The retention times of [ $^{11}\text{C}$ ]MBF and [ $^{11}\text{C}$ ]JP-1302 were 4.1 and 4.9 min, respectively. Radioactivity in the supernatants, residual precipitates after centrifugation, and waste solution from HPLC were measured using an automatic  $\gamma$  counter. Percentages of the unchanged form were then determined.

### **PET Study in Mice**

PET scans were obtained using an Inveon dedicated PET scanner (Siemens Medical Solutions, Knoxville, TN). P-gp/Bcrp knockout mice (age, 31–34 weeks; weight, 34–38 g;  $n = 3$  per tracer) and wild-type mice (age, 11–14 weeks; weight, 26–43 g;  $n = 3$  per tracer) were used in the PET study.

Mice were anesthetized with isoflurane (1.0–1.5%, v/v) and placed in a prone position on the bed. [ $^{11}\text{C}$ ]MBF (4.1–7.8 MBq/0.12–1.22 nmol) or [ $^{11}\text{C}$ ]JP-1302 (3.6–8.1 MBq/0.033–0.078 nmol) was intravenously injected into mice. A time sequential scan was carried out for 60 min in the three-dimensional (3D) list mode with an energy window of 350–650 keV. List-mode data were sorted into 3D sinograms (6  $\times$  10 s, 4  $\times$  15 s, 5  $\times$  1 min, 4  $\times$  2 min, 3  $\times$  5 min, and 3  $\times$  10 min), which were then Fourier rebinned into two-dimensional sinograms. Dynamic images were reconstructed with filtered back-projection using a ramp filter. Decay-corrected radioactivity was expressed as SUV. Regions of interests (ROIs) were masked on the brain using ASIPro VM software (Siemens Medical Solutions). The area under the time–activity curve of the ROIs in the brain (AUC<sub>brain</sub>, SUV  $\cdot$  min) was calculated starting from 0 to 60 min.

### **Statistical Analysis**

Quantitative data are expressed as the mean  $\pm$  standard deviation (SD). In the *in vivo* distribution study, differences between control and treatment groups were tested by one-way analysis of variance (ANOVA) and Dunnett's *post hoc* tests. In the *in vivo* distribution study, different groups were assessed using one-way ANOVA and Bonferroni's multiple comparison tests. The data was analyzed using GraphPad Prism 5 software (GraphPad Software, San Diego, CA). Differences were considered significant if  $P < 0.05$ .

## **Supporting Information Available**

HPLC results for compounds **6** and **11** and MBF. This material is available free of charge via the Internet at <http://pubs.acs.org>.

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### Author Contributions

Drs. Ming-Rong Zhang and Toshimitsu Fukumura designed compounds and directed the synthetic chemistry experiments, synthetic radiopharmaceutical chemistry experiments, and molecular imaging. Drs. Megumi Akiyama and Katsushi Kumata performed synthetic chemistry experiments and radiopharmaceutical chemistry experiments. Drs. Joji Yui, Tomoteru Yamazaki, Akiko Hatori, Kazuhiko Yanamoto, and Hidekatsu Wakizaka performed the *in vivo* biology experiments and molecular imaging. Drs. Makoto Takei and Nobuki Nengaki performed synthetic radiopharmaceutical chemistry experiments.

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